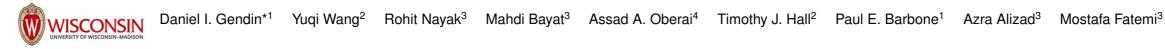
Repeatabilty of mechanical property maps in breast tumors







¹ Boston University, ² University of Wisconsin, ³ Mayo Clinic College of Medicine and Science, ⁴ University of Southern California

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Breast cancer statistics

- Excluding skin cancer, breast cancer is the most common cancer in
- Breast accounts for 1/3 of cancers found in women.
- Breast Cancer is the 2nd leading cause of cancer death among women (after lung cancer).
- Breast masses present as stiff lumps, and hence are known to have pathological mechanical properties.

TABLE 2.	Age-Specific Probabilities of Developing Invasive Female Breast Cancer ^a	

IF CURRENT AGE IS:	THE PROBABILITY OF DEVELOPING BREAST CANCER IN THE NEXT 10 YEARS IS:	
20	0.06%	1,732
30	0.44%	228
40	1.45%	69
50	2.31%	43
60	3.49%	29
70	3.84%	26
Lifetime risk	12.29%	8

Statistics from [2]

Desmoplastic effect

• The stiffness of tumors is likely due to the desmoplastic effect, in which excessive connective tissue (stroma) forms around an invasive tumor [1].

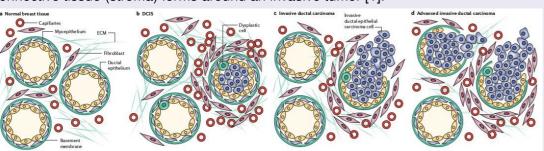
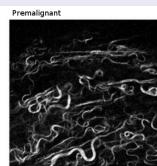
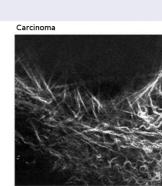


Illustration of desmoplasia from: [5]

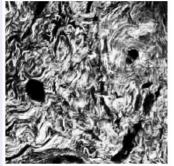
- The morphology of the connective tissue (collagen fibers) around the tumor depends on the tumor nature.
- SHG images of collagen fibers from breast tissue.

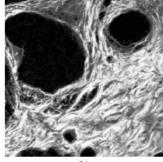


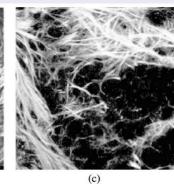




Source: [3]







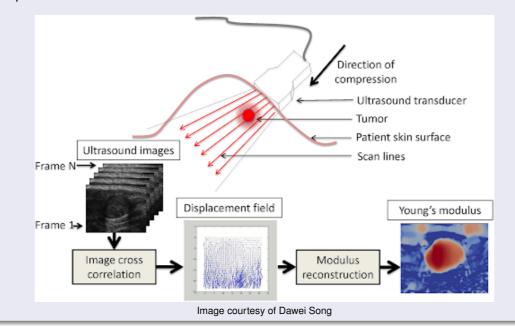
Malignant

Figure 1. SHG images of (a) normal, (b) benign and (c) malignant breast tissue. Differences in the collagen fibre shape are evident between tissue groups

• The changes in tissue structure and morphology on the micro-scale changes the behavior and properties of tissue on the mm scale.

Imaging material properties

• Bayesian inversion from ultrasound image sequences coupled with a mathematical model of tissue deformation allows us to make images of breast tissue mechanical



Mechanical Model

• Veronda-Westmann [6] strain energy function(incompressible,plane stress):

$$W = \mu \left(\frac{e^{\gamma(l_1 - 3)} - 1}{\gamma} - \frac{l_2 - 3}{2} \right) \tag{2}$$

$$\mathbf{S} = \mu \bigg(2e^{\gamma(l_1+1/l_2-3)} \big(\mathbf{I} - \frac{1}{l_2} \mathbf{C}^{-1} \big) - \frac{1}{l_2} \mathbf{I} - (l_2 - \frac{l_1}{l_2}) \mathbf{C}^{-1} \bigg)$$

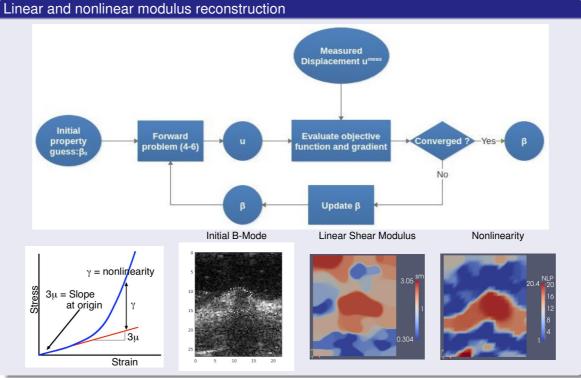
Objective function

$$C[\beta] = \int_{A} (u_{y}(\beta) - u_{y}^{meas})^{2} dA + \alpha \int_{A} \sqrt{|\nabla \beta|^{2} + c^{2}} dA$$
(3)

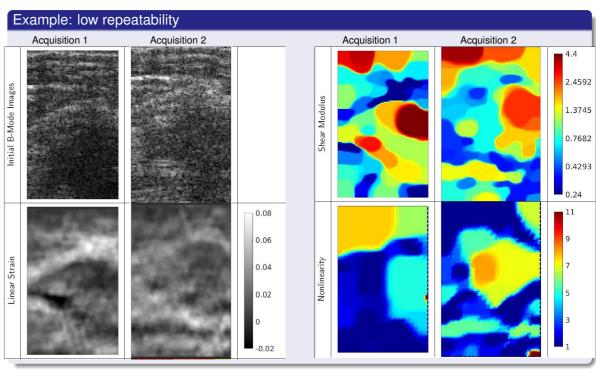
Here β is a material parameter (either the linear shear modulus μ or the non-linearity

Governing equations and boundary conditions

$$\nabla \cdot (\mathbf{FS}) = 0 \text{ on } \Omega_0 \quad (4)$$
 $u_V = u_V^{meas} \text{ on } \partial \Omega_0 \quad (5)$ $t_X = 0 \text{ on } \partial \Omega_0. \quad (6)$



Example: high repeatability Acquisition 1 Acquisition 2



Discussion and conclusions

- Changes in tissue at the micro level, result in alterations to behavior and properties at
- Mechanical property images can serve as adjunct images to potentially improve diagnosis at screening time.
- We studied the repeatability of our reconstructions using data from patients who were imaged multiple times.
- When acquisitions represent similar regions of tissue (as measured by correlation between initial ultrasound images) the resulting mechanical property reconstructions are highly repeatable.
- When acquisitions represent different regions (or imaging planes) of tissue the resulting reconstructions are less repeatable.
- When insufficient strain is applied to adequately observe nonlinear behavior, the resulting nonlinearity reconstructions could exhibit very low repeatability.
- Repeatability of nonlinearity can vary noticeably with processing parameters.

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