

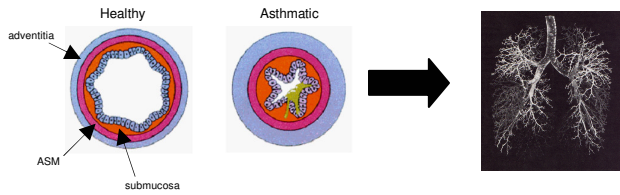
## INTRODUCTION

### Airways

- The airway tree is a complex 3-D structure with non-symmetric bifurcations
- Mechanics of individual airways, such as pressure-area relationships and compliance, are important because they integrate to affect whole lung function

### Asthma

- Airway disease characterized by inflammation, thickening of the airway walls, and luminal secretions
- All three layers of the airway wall (adventitia, airway smooth muscle, and submucosa) become thicker in asthma
- Causes reduction in airway diameter, increased airway resistance, and hyperresponsiveness to a range of stimuli



Pictures from Lewis, 2002.

## RATIONALE

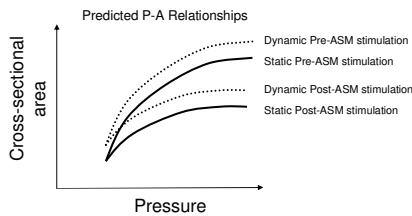
### Past Work on Isolated Airways and ASM

- Previous studies have examined the *static* pressure-area relationships of isolated airways<sup>1</sup>
- Dynamic length cycling of ASM causes it to remodel so as to generate less force than when held at a static length<sup>2</sup>
- Breathing is a dynamic process

➔ An isolated airway with intact ASM examined dynamically will produce pressure-area relationships that more accurately represent the impact of breathing on wall mechanics

### Dynamic Pressure-Area (P-A) Relationships

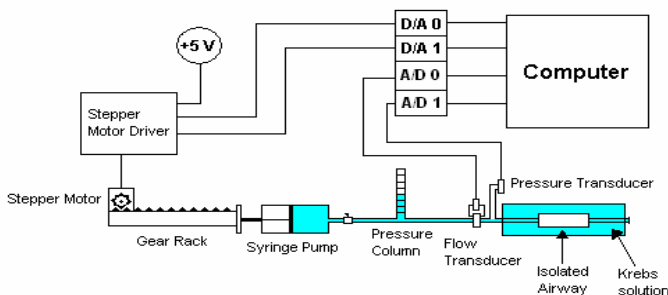
- As with static P-A relationships, healthy airways should have a higher cross-sectional area than stimulated airways
- Dynamic P-A curves should have a higher CSA than static P-A curves because ASM becomes more plastic when dynamically oscillated
- The slope will be greater for pre-stimulated airways because of a higher compliance



## SPECIFIC AIMS

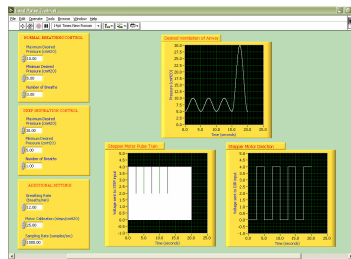
- To develop a system to study the dynamic properties of isolated airways with intact ASM
- System must produce the appropriate pressure changes across the airway wall to simulate normal breathing and deep inspirations
- System must be:
  - User-friendly
  - Computer-controlled
  - Adaptable, in order to produce different breathing patterns

## SYSTEM OVERVIEW



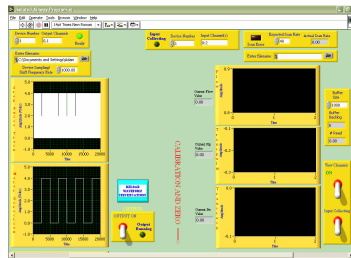
- The system functions as follows:
  - A computer-controlled stepper motor drives a syringe pump
  - The syringe pumps Krebs solution into and out of a pressure column
  - The height of the pressure column determines the pressure of the Krebs solution that is delivered into the isolated airway
  - The pressure and flow going into the airway are measured
- Additional notes:
  - Airway transmural pressure is the independent variable
  - For a normal breathing case, the system should deliver pressures of 5 to 10 cmH<sub>2</sub>O in a sinusoidal manner into the isolated airway
  - Rigid tubing is used to ensure that the system compliance does not effect the measured pressure and flow

## SOFTWARE



### Program 1 – Creating Desired Pressure Waveform

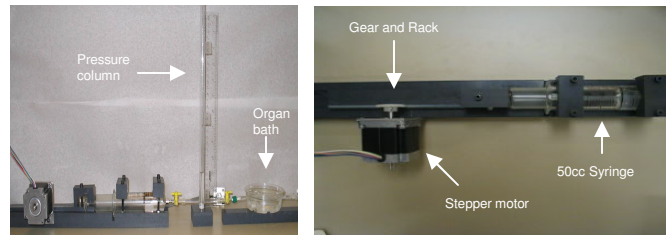
- Labview GUI
- Allows user to make a desired sinusoidal pressure waveform to simulate breathing (5 to 10 cmH<sub>2</sub>O for normal breaths; 5 to 25 cmH<sub>2</sub>O for deep inspirations)
- Translates waveform into a corresponding pulse train and step function that drives the stepper motor driver



### Program 2 – Outputting Waveform and Collecting Data from Transducers

- Labview GUI
- Outputs pulse train and step function to stepper motor driver
- Inputs and records flow and pressure data from transducers

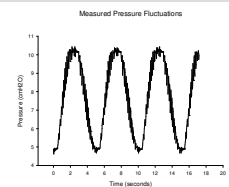
## HARDWARE



- The side and top view of the system show (from left to right): the stepper motor, the gear and gear rack, the 50cc syringe, the pressure column, and the organ bath

## INITIAL TESTING

- Initial testing has shown that the pressures delivered past the pressure column are sinusoidal and oscillate in the correct range
- Some noise is present due to the stepping of the stepper motor



## PROJECT END GOAL

- Perform experiments using airways excised from calf lungs
- Using the sampled pressure and flow data, determine the following relationships for pre- and post-activated ASM:
  - Transmural Pressure and Cross-sectional Area
 
$$V_{aw} = \int Flow dt \quad CSA = V_{aw} / Law$$
  - Transmural Pressure and Compliance
 
$$Compliance = dV_{aw} / dP_{tm}$$
- Improve 3-D computer lung models using dynamic pressure-area relationships

Where:  
P<sub>tm</sub> = transmural pressure (cmH<sub>2</sub>O)  
V<sub>aw</sub> = airway volume (cm<sup>3</sup>)  
Law = airway length (cm)  
CSA = airway cross-sectional area (cm<sup>2</sup>)

## REFERENCES

- Gunst, S.J., and J.Q. Stropp, *Pressure-volume and length-stress relationships in canine bronchi in vitro*. American Physiological Society, 1988. 88: 2522-2531.
- Latourelle, J., B. Fabry, and J.J. Fredberg, *Dynamic equilibration of airway smooth muscle contraction during physiological loading*. J Appl Physiol, 2002. 92: 771-779.

## ACKNOWLEDGEMENTS

Partially funded by a grant from the National Science Foundation (NSF-REU) to Boston University.