

# Tracking lineages of single cells in lines using a microfluidic device

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Cells within a genetically identical population exhibit phenotypic variation that in some cases can persist across multiple generations. However, information about the temporal variation and familial dependence of protein levels remains hidden when studying the population as an ensemble. To correlate phenotypes with the age and genealogy of single cells over time, we developed a microfluidic device that enables us to track multiple lineages in parallel by trapping single cells and constraining them to grow in lines for as many as 8 divisions. To illustrate the utility of this method, we investigate lineages of cells expressing one of 3 naturally regulated proteins, each with a different representative expression behavior. Within lineages deriving from single cells, we observe genealogically related clusters of cells with similar phenotype; cluster sizes vary markedly among the 3 proteins, suggesting that the time scale of phenotypic persistence is protein-specific. Growing lines of cells also allows us to dynamically track temporal fluctuations in protein levels at the same time as pedigree relationships among the cells as they divide in the chambers. We observe bursts in expression levels of the heat shock protein Hsp12-GFP that occur simultaneously in mother and daughter cells. In contrast, the ribosomal protein Rps8b-GFP shows relatively constant levels of expression over time. This method is an essential step toward understanding the time scales of phenotypic variation and correlations in phenotype among single cells within a population.

epigenetics | protein expression | single cell assay | yeast

Nearly 150 years ago, Mendel elucidated the fundamental unit of heredity by tracing and applying statistics to inheritance patterns in pea plants. In most cases, heritable phenotypic variation arises from differences in DNA sequence, yet even cells that are genetically identical can exhibit distinct, heritable states that are critical during differentiation and development, and possibly in response to environmental stress. Phenotypic variation that occurs on time scales shorter than the characteristic cell division time is known to result from the stochastic processes inherent to gene and protein expression (1). However, variations in protein levels at frequencies longer than the typical generation time enable phenotypic states to be passed on to genetically identical progeny cells, a phenomenon known as epigenetic inheritance (1, 2); the time scales of such multigenerational variation are less well understood. Mechanisms that generate phenotypic variation that propagates over many cell divisions include positive feedback loops in genetic networks (3–5), protein aggregation (6), and chromatin state (2, 7). Phenotypic variation may provide a fitness advantage for a population of cells in a fluctuating environment (8), and the ability to inherit phenotype is proposed to benefit populations in conditions in which the environment changes on time scales faster than genetic mutations occur (9). Such bet-hedging in microbial populations may have medical consequences: for example, a subset of “persistence” cells within an actively growing population of bacteria divides more slowly and shows increased antibiotic resistance (10). Despite the importance of epigenetic mechanisms of gene regulation, the time scales of variation at the single cell level remain poorly understood.

To study the phenotype of single cells in the context of pedigree demands a method to collect data over many cells and over many generations. The budding yeast, *Saccharomyces cerevisiae*, is a good model eukaryotic system: yeast cells divide rapidly, making it technically feasible to study multiple generations of cells. Proteome-wide studies of *S. cerevisiae* have characterized stationary distributions of protein levels across a population by microscopy and flow cytometry, revealing that expression of stress-related genes tends to be more variable (“noisy”), whereas housekeeping genes exhibit less cell-to-cell variation (11–14). However, these measurements capture neither changes in expression over time nor correlations in protein levels resulting from age or pedigree relationships among individuals. To characterize cells and their progeny requires following single cells and their offspring during growth; this can be achieved by individually separating cells by micromanipulation (15) or by imaging cells as they grow sandwiched between an agar pad and a cover glass (5). However, manual manipulation of cells is laborious, and accurately determining pedigree and protein expression by microscopy is challenging as cells grow out of the focal plane after only a few divisions. Various microfluidic devices maintain cells in a single focal plane as they grow (10, 16–21), but many of these devices require sophisticated fabrication techniques such as multilayer fabrication with valves (16, 18), channel height differences (17), or membranes (10, 21). To optimize the statistical power of these techniques, the initial placement of cells should be controlled; several other microfluidic devices achieve single-cell trapping (22–24), but these trapping mechanisms are not conducive to the lineage analysis that we perform here. The ability to robustly and repeatedly trap, spatially organize, and track the growth of single cells over many generations in a device that is easy to fabricate and simple to use would enable the collection of data over many cell lineages in a single experiment.

Here we introduce a simple microfluidic device for following lineages deriving from single yeast cells. We seed single parental cells into channels fabricated at a high density to maximize the number of lineages tracked in each experiment. To simplify tracking both pedigree and levels of protein expression, we geometrically constrain the cells to divide in a line within a single focal plane. Furthermore, we design the device so that fluid can constantly perfuse through the device, which allows us to replenish media, change environmental conditions, and perform other analyses. For example, we are able to fix and stain the cells in situ. By studying protein expression in the context of pedigree, we are able to see patterns of expression where phenotype is correlated over multiple

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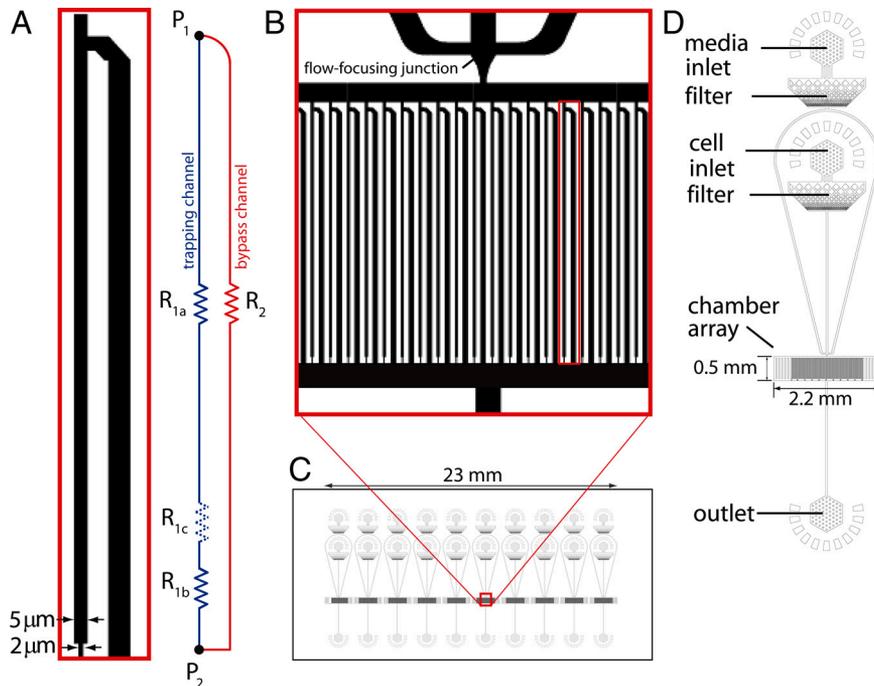
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**Fig. 1.** Lineage chamber device layout. (A) A single chamber consists of a long channel with a 5- $\mu\text{m}$  width and a 2- $\mu\text{m}$  constriction, as shown in this inset of B. The flow patterns can be understood in terms of an electrical circuit, with  $R_{1a}$ , the resistance of the trapping chamber;  $R_{1b}$ , the resistance of the constriction;  $R_{1c}$ , the resistance of a single cell; and  $R_2$ , the resistance of the bypass channel. The pressure drop ( $P_1 - P_2$ ) is equivalent for both fluid paths. (B) The chamber array consists of 50 chambers arranged in parallel, approximately half of which are active and shown in this inset of C. A flow-focusing geometry centers the flow of the cells into the chamber array. (C) Ten individual devices fit onto a 50  $\times$  24-mm coverslip enabling multiple conditions or cell types to be tested in a single experiment. (D) Overview of the entire lineage chamber device. Two inlets allow for separate flow paths of the cell suspension and media. Filters eliminate aggregates of cells.

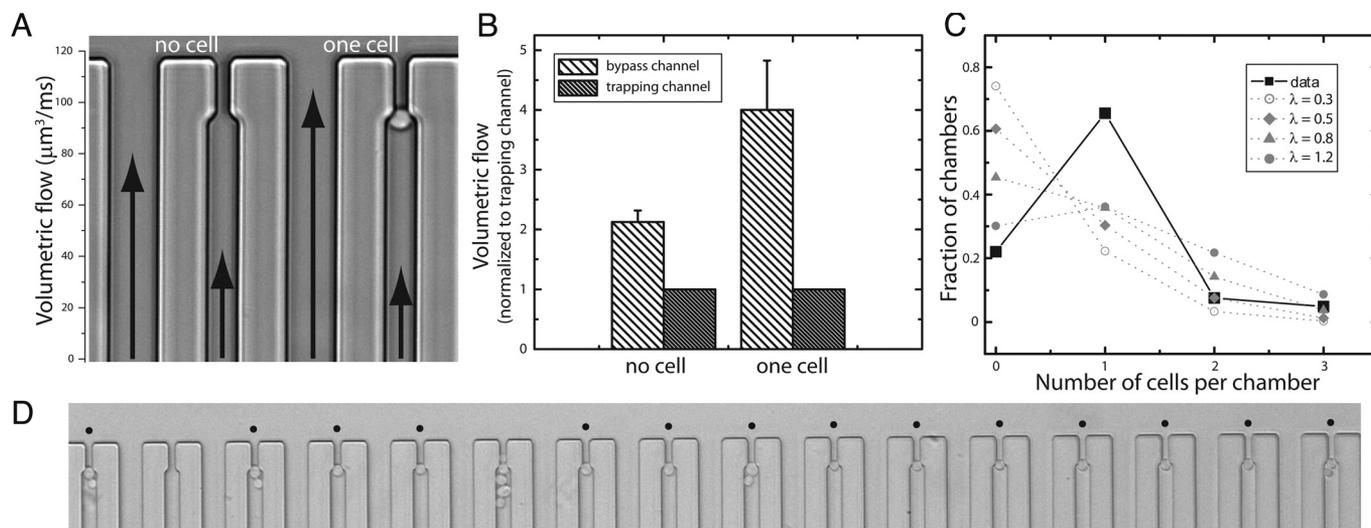
generations; such information remains hidden when studying at the population as an ensemble.

**Device Concept.** To facilitate analysis of single cells and their progeny, we designed a microfluidic device in which lineages deriving from single cells are spatially organized in lines. For nearly a century, linear arrays of spores encapsulated in natural, rod-shaped ascus sacs have proven useful for elucidating the mechanisms of Mendelian inheritance (25); more recently, lineages of bacterial cells in lines have been studied in microfluidic devices (10). However, when placing cells in chambers of a fabricated device, the distribution of cells is random, with the number of cells per chamber dictated by Poisson statistics. To achieve a high proportion of single cells seeded in the linear chambers, we fabricated an array of chambers that have a constriction at one end, so cells are trapped when they flow into the chambers (Fig. 1A). After one cell enters a chamber, the ratio of flow through the chamber to bypass channels shifts, increasing the probability that subsequent cells preferentially enter the bypass channel instead of the growth chamber (26). Importantly, our device is easily fabricated by using a single cast of polydimethylsiloxane (PDMS) and requires only a syringe pump and microscope for operation.

To understand the single cell trapping mechanism, we estimate the flow rate through the microfluidic device by using lumped element modeling, an approach often used to analyze simple electrical circuits. The volumetric flow rate,  $Q$ , through the channels is analogous to electrical current; the pressure drop,  $\Delta P$ , is analogous to the voltage drop; and the remaining factors describe the fluidic resistance that depends largely on the channel geometry. The trapping (Fig. 1A, blue) and bypass (Fig. 1A, red) channels act as 2 lumped resistors in parallel; the pressure drop across both channels must be equal because the end points are the same,  $\Delta P_1 = \Delta P_2$  (Fig. 1A). For efficient single cell trapping, the presence of a cell in the trapping channel should change the flow such that

subsequent cells do not enter. Thus, when the trapping channel is empty, the flow through the bypass channel,  $Q_2$ , should be less than the flow through the trapping channel,  $Q_1$ ; when a single cell is present in the channel,  $Q_2$  should be greater than  $Q_1$  so that most of the flow, and therefore subsequent cells, flow through the bypass channel (27). We design the device given this criterion and other geometric requirements, as outlined in the *SI Text*. For example, to spatially organize the microcolonies that derive from the array of single cells and force them to grow in a single focal plane, we engineered the growth chambers with a square cross-section that is the width and height of an average single cell,  $w_{1a} = h_2 = h_{1a} = 5 \mu\text{m}$ .

Given these prerequisites, we designed the device with an array of 50 chambers (Fig. 1D); roughly half of these are active chambers that fill with cells (Fig. 1B). Because 10 or more devices can be fabricated on each chip (Fig. 1C), hundreds of cells can be trapped, enabling the simultaneous testing of different flow conditions or cell types in a single experiment. We loaded cells into the device by activating 2 syringes that contain the cell suspension and growth media (Fig. 1D and Fig. S1). To provide greater control between the 2 fluid streams, we fabricated a flow-focusing junction at the entry to the chamber array: the cells flow down the center while the media flows in from the sides (Fig. 1B). This geometry prevents cells from flowing into the media line, and thus maintains a cell-free source of media for perfusion during the experiment. When single cells are loaded, we deactivate the cell-loading inlet by disconnecting the tubing from the syringe. To allow for metabolite exchange during cell growth, we continually flow media through the device during the experiment; as the cells are round and the channels are square, media perfuses through the chambers as cells grow. The continued media flow also ensures there is constant flow backward through the cell inlet, preventing cells trapped upstream from entering the chamber array (Fig. S1).



**Fig. 2.** Trapping single cells in the lineage chambers. (A) Average volumetric flow rates through the bypass and trapping channels are proportional to the length of arrows superimposed on this bright-field image. Flow through the bypass channel doubles when a single cell is trapped, increasing the probability for cells to flow through the bypass while still allowing for fluid flow through the trapping channel. (B) Volumetric flow through the bypass channel normalized to the trapping channel. Error bars represent SD for  $n = 6$  (bypass) and  $n = 9$  (trapping) channels. (C) After loading, there are 0.8 cells per active chamber. Data shown here are summed over 30 independent experiments. Plotting an equivalent Poisson distribution ( $\lambda = 0.8$ ) would result in less than 40% chambers containing single cells (gray triangles), as well as chambers that are empty or contain multiple cells. Other gray symbols represent Poisson distributions for other  $\lambda$  values. (D) Bright-field image showing an array of trapping chambers filled with single cells that are identified by black dots. (Channel width,  $5 \mu\text{m}$ .)

## Results and Discussion

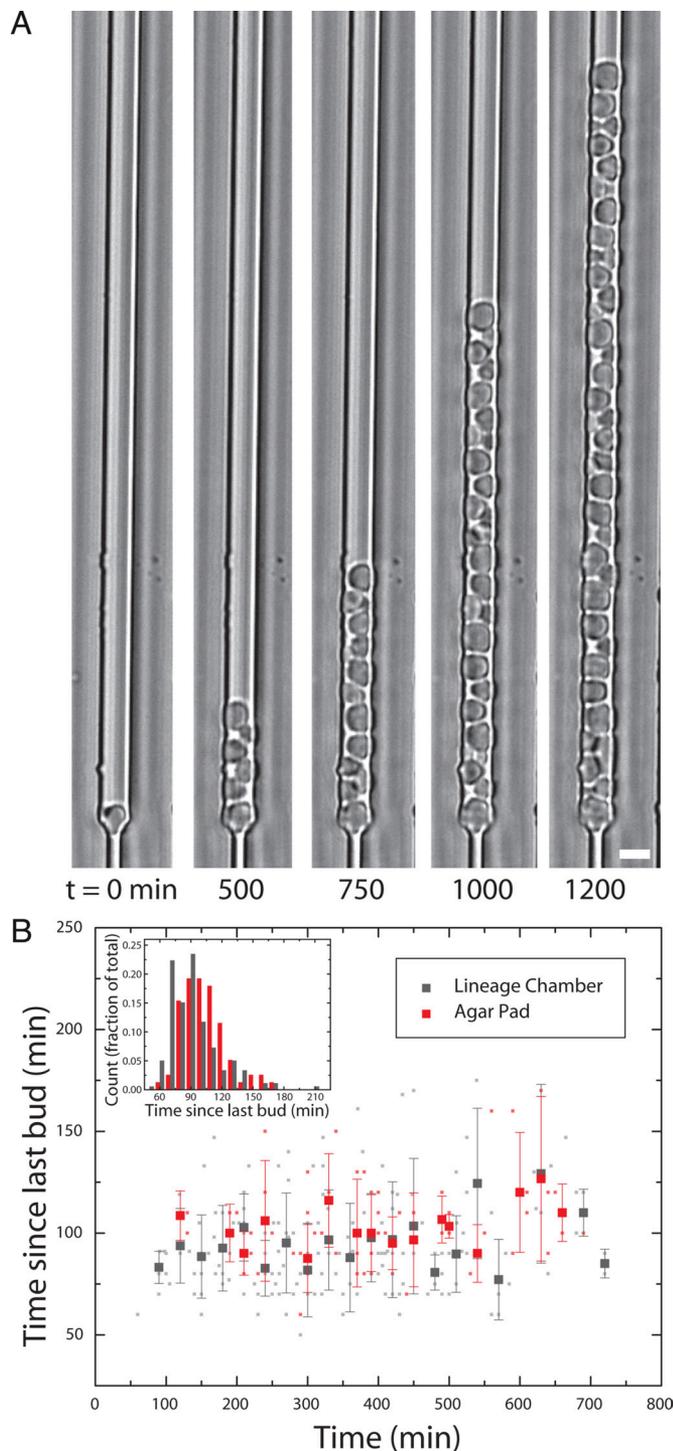
To demonstrate our single cell trapping mechanism, we measure the flow through the chamber and bypass channels by imaging tracer particles: when the trapping channel is empty, the volumetric flow through the bypass channel,  $Q_2$ , is approximately twice that through the trapping channel,  $Q_1$ :  $Q_2/Q_1 = 2.1 \pm 0.2$  ( $n = 6$ ; Fig. 2A and B). This value is in excellent agreement with simple estimates of flow when the trapping chamber is empty (Eq. 1 and *SI Text*). Thus, while cells are loading, many of them pass through the bypass channel, and some cells flow into the chambers. However, when a single cell is trapped in the lineage chamber channel, the flow through the bypass channel increases to  $Q_2/Q_1 = 4.0 \pm 0.8$  ( $n = 9$ ; Fig. 2A and B) as a result of the decrease in the cross-sectional area of the trapping channel. The resulting change in fluidic resistance upon trapping a single cell increases the probability that additional cells are diverted through the bypass channel instead of the trapping channel. Importantly, the continued flow even in the presence of a trapped cell allows for media exchange during cell growth.

With this method, device loading is complete within 2 to 3 min with good single cell trapping efficiency: on average, 70% of the active chambers fill with single cells (Fig. 2C and D). The majority of the remaining chambers are empty, and some contain multiple cells. If the loading of cells were completely random and independent of the number of previously trapped cells, the number of cells per chamber would follow a Poisson distribution whereby, for the same average number of cells trapped per chamber, the majority of chambers would be empty, only 40% would have single cells, and a smaller number would contain multiple cells (Fig. 2C); our loading mechanism thus achieves much better efficiency than dictated by Poisson statistics. Note that deviations from ideal loading with 100% single cells may result from the low flow ratio between bypass and trapping channels (27), variations in cell size, asymmetry in cell shape, or differences in cell stiffness that may affect the extent to which a cell deforms into the constriction and blocks the channel.

As the cells divide in the long, narrow growth chamber, they are constrained to grow in a line. To evaluate growth of cells in the lineage chambers, we acquire images of cells at 10-min intervals

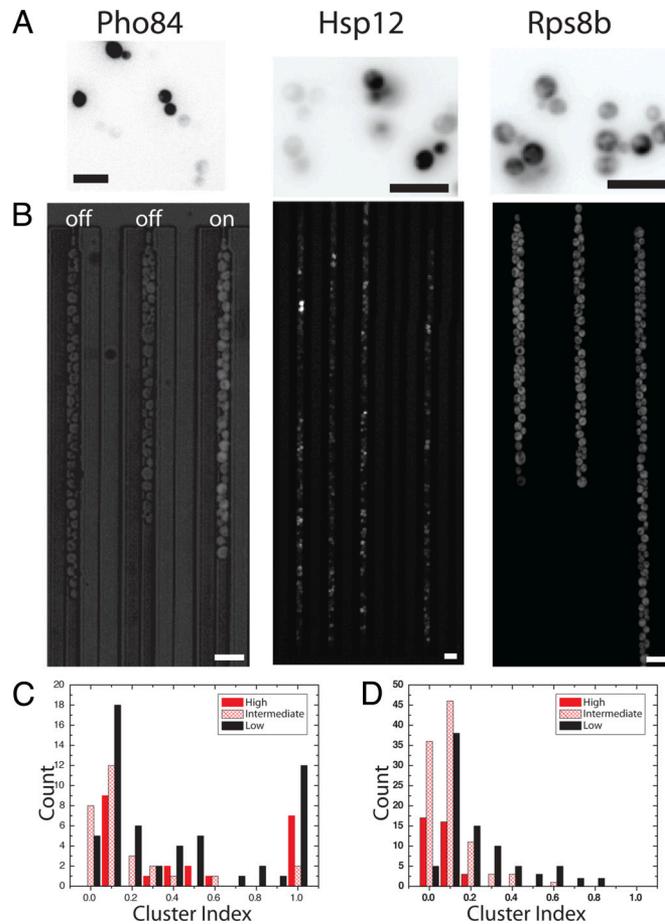
(Fig. 3A). We compare growth of cells in chambers to those on agar pads, a common method for time-lapse imaging of yeast cells. Analysis of the time between buddings for single cells shows that doubling time is similar for cells cultured in the lineage chambers and on agar pads (Fig. 3B). For a given cell, we observe a relatively constant division time over the course of the experiment even for cells at the bottom of the chamber. To determine if media exchange is hindered by an increasing number of cells per chamber, we flow a solution containing fluorescent probe through chambers filled with cells. We observe that all cells along the channel become fluorescently labeled, showing that liquid penetrates around cells along the length of the channel, and confirming that fluid exchange happens on the order of minutes (Fig. S2).

We analyze lineages of cells by using the device in one of 2 ways: in endpoint mode, in which we acquire a single image at the end of the growth experiment, or in kinetic mode, in which we quantitatively track protein levels in single cells over time. To illustrate the utility of the device, we investigate the expression of 3 representative proteins, each with a distinct expression pattern. As an example of endpoint mode, we first study the expression of the protein Pho84, a high-affinity phosphate transporter, whose expression is subject to positive feedback and exhibits bimodal expression when cells are grown in intermediate phosphate concentrations (28). Expression of Pho84 is expected to switch between the “on” and “off” phenotypic states at some frequency; yet from images of cells in bulk acquired at a single time point (Fig. 4A), or from the stationary distribution obtained by flow cytometry (Fig. S3) (28), the time of switching between states cannot be determined. To address this question, we image cells expressing pPho84-GFP after growth in the lineage chambers. Each line represents a lineage deriving from a single cell with domains of cells that are closely related genealogically (Fig. 5, gray bars). The frequency of phenotypic variation is easily determined by visually inspecting the lines of cells, and can be quantified with simple image analysis. In some cases, entire lineages of cells have a similar phenotype, with either uniformly high or low Pho84 levels (Fig. 4B). We interpret these lineages as resulting from seeding by a single “on” or “off” cell; maintenance of the phenotypic state over multiple cell divisions results in an entire lineage with relatively uniform expression level.



**Fig. 3.** Cells grow in a line. (A) Single progenitor cells are constrained to grow in a line, as shown in this time sequence of bright-field images. (B) Doubling times are similar for cells grown in lineage chambers ( $n = 180$ ) versus on agar pads ( $n = 78$ ). Hsp12-GFP cells in YPD media. *Inset*, histogram of doubling times. Bin size, 10 min. (Scale bar,  $5 \mu\text{m}$ .)

We also observe clusters of adjacent cells within a lineage that are either “on” or “off,” which result from a change in expression state during lineage growth. We quantify the number of cells per cluster, normalize to the number of cells in the lineage to obtain a “cluster index” (CI), and plot the CI distribution (Fig. 4C). When the CI is 1, all cells within an entire lineage have similar protein levels, whereas a CI less than 1 indicates the presence of clusters of cells



**Fig. 4.** Phenotypic variation in lineages of cells. Three different proteins, pPho84-GFP, Hsp12-GFP, and Rps8b-GFP, as seen by inverted GFP-fluorescence images (A) and after growth in lineage chambers (B). We observe lines of high- or low-expressing pPHO84-GFP cells in intermediate phosphate concentration ( $200 \mu\text{M}$  phosphate), suggesting that a particular phenotypic state is maintained over multiple divisions. By contrast, the heat shock protein Hsp12-GFP shows smaller clusters, indicating that protein levels change on a relatively faster time scale. Cells that express the ribosomal protein Rps8b-GFP show little variation along lineages. Images are sequentially thresholded to identify cells with similarly high, intermediate, or low fluorescence. The cluster index (CI) is the number of adjacent cells with similar fluorescence divided by the total number of cells in a lineage, and provides a qualitative measure of the number of generations that protein levels persist. CI distributions for  $n$  individual cells for (C) pPHO84-GFP ( $n = 1,309$  from 38 tracks); (D) Hsp12-GFP ( $n = 1,122$  from 33 tracks). (Scale bar,  $10 \mu\text{m}$ .)

that each have a distinct phenotype. Importantly, we observe that clusters form at all positions along the chambers, and that expressing cells may be adjacent to or upstream from non-expressing cells; if cell-cell communication by soluble factors determined protein expression patterns, cells downstream from or adjacent to expressing cells would consistently exhibit similar protein levels. This very simple experiment thus shows that we can detect the persistence of a particular phenotypic state over multiple generations, and thereby demonstrates the efficacy of our system for the study of cell lineages.

We next investigate the behavior of 2 representative proteins that show unimodal bulk distributions, but with different variances: the heat shock protein Hsp12 belongs to a family of stress proteins that exhibit large variation in expression levels compared with essential “housekeeping” proteins such as the ribosomal protein Rps8b (Fig. S3) (13, 14). Indeed, imaging the Hsp12-GFP cells in bulk at a single time point shows that some cells are very bright whereas others express low levels of protein (Fig. 4A); however, it is not known how expression levels fluctuate over time. Growing Hsp12-GFP cells in



that propagate in single cells over time and over multiple generations. In addition, it is possible to study any asymmetries at cell division, correlations between cells caused by their pedigree, replicative age, or any other physical trait such as volume. The pedigree analysis software is generally applicable to any yeast strain, and does not require additional fluorescent markers for progeny identification. A further benefit of our device is the ability to fix and stain single suspension cells and their lineages, allowing morphological phenotypes on subcellular scales to be resolved, for example, by immunofluorescence or FISH. With slight modifications in size, the lineage chambers can also be used for culture of other suspension cells, including mammalian blood cells or stem cells. More broadly, our device will enable studies revealing correlations among single cells and their progeny that remain masked in the ensemble average.

## Materials and Methods

**Lumped Element Modeling.** For a rectangular channel, the relationship between the pressure drop  $\Delta P$  and flow rate  $Q$  is given by the Hagen-Poiseuille relation,  $\Delta P = 12Q\eta/h^3w$ , where  $\eta$  is the dynamic viscosity and  $w$ ,  $h$ , and  $l$  are the channel width, height, and length. The bypass channel is considered as a single resistor,  $R_2$ , with dimensions  $w_2$ ,  $h_2$ , and  $l_2$ . The trapping channel consists of 2 resistors:  $R_{1a}$ , the long channel with dimensions  $w_{1a}$ ,  $h_{1a}$ , and  $l_{1a}$ ; and  $R_{1b}$ , the narrow constriction neck with dimensions  $w_{1b}$ ,  $h_{1b}$ , and  $l_{1b}$  (Fig. 1A). The ratio of flow through the bypass to trapping channel is expressed as follows:

$$\frac{Q_2}{Q_1} = \frac{R_{1a} + R_{1b}}{R_2} = \frac{h_2^3 w_2}{l_2} \left[ \frac{l_{1a}}{h_{1a}^3 w_{1a}} + \frac{l_{1b}}{h_{1b}^3 w_{1b}} \right] \quad [1]$$

**Microfluidic Device Fabrication.** Soft lithography is used to fabricate microfluidic channels in PDMS (Sylgard 184 silicone elastomer; Dow Corning) (38). Devices are

bonded to Lab-tek II 2-well chambered cover glass (no.1.5 borosilicate glass; Nalge Nunc no. 62407-052; Thermo Fisher Scientific).

**Yeast Cell Culture.** Cell strains are from the GFP-library (Invitrogen). The pPHO84-GFP strain (w303, MATa, pPHO84-yeG::URA3) is a generous gift from the lab of Erin O'Shea (Cambridge, MA). Liquid cultures are inoculated from a single colony into yeast extract/peptone/dextrose (YPD) or intermediate phosphate concentration media (39) and are shaken at room temperature for 24 h to a density of  $2$  to  $6 \times 10^5$  cells/mL.

**Device Operation.** Syringe pumps (Harvard Apparatus) control fluid flow. To track flow velocities through the channels, we flow  $0.465\text{-}\mu\text{m}$  polystyrene beads (Polysciences) through the device at  $5 \mu\text{L/h}$  and acquire images at 5,000 frames per second with a high-speed camera (Phantom v7.3; Vision Research).

**Growth Rates.** Agar pads are made by molding 1.5% wt/wt agar in YPD between 2 glass slides separated by a rubber spacer (Grace Bio-Labs; Sigma).

**Imaging.** We acquire images of cells every 10 min by using an inverted microscope equipped with an automated stage (Prior Scientific),  $\times 20$  objective, and GFP filter set.

**Image Analysis.** CI analysis is performed by twice sequentially thresholding the endpoint image to identify adjacent cells with high, intermediate, and low fluorescence. To construct complete lineage maps, we acquire a bright field and fluorescence image at 10-min time intervals and track cells using custom MATLAB software (MathWorks).

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